

Relationship Between the Ambulatory Arterial Stiffness Index and the Lower Limit of Cerebral Autoregulation During Cardiac Surgery

Yurie Obata, MD; Viachaslau Barodka, MD; Dan E. Berkowitz, MD; Allan Gottschalk, MD, PhD; Charles W. Hogue, MD; Jochen Steppan, MD, DESA

Background—Pulse pressure, the ambulatory arterial stiffness index (AASI), and the symmetric AASI are established predictors of adverse cardiovascular outcomes. However, little is known about their relationship to cerebral autoregulation. This study evaluated whether these markers of vascular properties relate to the lower limit of cerebral autoregulation (LLA).

Methods and Results—The LLA was determined during cardiac surgery with transcranial Doppler ultrasonography in 181 patients. All other variables were calculated from continuous intraoperative readings obtained before cardiopulmonary bypass. The LLA varied directly with the AASI ($\beta=3.12$ per 0.1 change in AASI, $P<0.001$) and to a lesser extent the symmetric AASI ($\beta=2.02$ per 0.1 change in symmetric AASI, $P\leq 0.022$), while peripheral pulse pressure was not significantly related ($\beta=0.0$, $P>0.99$). Logistic regression revealed that the likelihood of LLA being >65 mm Hg increased by 50% (95% confidence interval, 11%–102%, $P=0.008$) for every 0.1 increase in the AASI. The AASI was able to predict a LLA above certain thresholds (area under the curve receiver operating characteristic for AASI predicting an LLA >65 mm Hg: 0.60; 95% confidence interval, 0.51–0.68%, $P=0.043$). Incorporating additional variables improved the model's predictive ability (area under the curve for AASI predicting a LLA >65 mm Hg: 0.75; 95% confidence interval, 0.68–0.82, $P=0.036$).

Conclusions—These data indicate that the LLA is related to the mechanical properties of the vasculature as represented by the AASI. The AASI can be used to predict LLA threshold levels during cardiac surgery. It is now possible to link elevations in the LLA with an increased AASI as determined from readily accessible intraoperative variables. (*J Am Heart Assoc.* 2018;7:e007816. DOI: 10.1161/JAHA.117.007816.)

Key Words: ambulatory arterial stiffness index • cardiac surgery • cerebral autoregulation • lower limit of cerebral autoregulation • pulse pressure

Preserved cerebral autoregulation and maintenance of systemic blood pressure within the cerebral autoregulatory range are key principles underlying the perioperative care of patients presenting for cardiac surgery and other procedures. In the perioperative setting, a substantial number of strokes result from tissue ischemia caused by inadequate cerebral perfusion throughout the perioperative period.¹ Similarly, it has been shown that the incidence of adverse neurologic outcomes is increased when cerebral perfusion

pressure is not maintained above the lower limit of cerebral autoregulation (LLA).² The LLA is defined as the pressure below which blood flow in the brain becomes pressure dependent, and is often assumed to be a mean arterial blood pressure (MAP) of 50 mm Hg.³ However, previous studies by our group have questioned this assumption and demonstrated that during surgery and anesthesia, the range for the LLA varies considerably between 40 and 90 mm Hg.⁴ Moreover, despite the commonly held presumption of such a relationship, no association has been established between preoperative MAPs and the LLA.⁴ To date, there are no reliable and widely used predictors of the LLA that can be derived from routine perioperative data, nor are there any commercially available methods to determine this limit in the clinical setting.

Both hypertension and arterial stiffness are risk factors for stroke.^{5–7} Furthermore, systolic hypertension and arterial stiffness are highly interdependent, and both are associated with increased pulse pressure (PP). We have shown previously that increased preoperative brachial PP is an age-independent predictor of stroke development after cardiac surgery.⁸ PP,

From the Department of Anesthesiology and Critical Care Medicine, Johns Hopkins University, Baltimore, MD (Y.O., V.B., D.E.B., A.G., J.S.); Department of Biomedical Engineering, Johns Hopkins University Baltimore, MD (D.E.B.); Department of Anesthesiology, Northwestern University Feinberg, Chicago, IL (C.W.H.).

Correspondence to: Jochen Steppan, MD, DESA, The Johns Hopkins University School of Medicine, Zayed Tower 6208, 1800 Orleans St, Baltimore, MD 21287. E-mail: J.Steppan@jhmi.edu

Received December 3, 2017; accepted January 5, 2018.

© 2018 The Authors. Published on behalf of the American Heart Association, Inc., by Wiley. This is an open access article under the terms of the Creative Commons Attribution-NonCommercial-NoDerivs License, which permits use and distribution in any medium, provided the original work is properly cited, the use is non-commercial and no modifications or adaptations are made.

Clinical Perspective

What Is New?

- This study investigates the relationship between the lower limit of cerebral autoregulation and vascular properties as quantified separately by the intraoperative ambulatory arterial stiffness index (AASI), the symmetric AASI, and peripheral pulse pressure in patients undergoing cardiac surgery.
- The AASI predicts the lower limit of cerebral autoregulation with a greater ability than the symmetric AASI; pulse pressure has no predictive ability.
- The lower limit of cerebral autoregulation is related to the mechanical properties of the vasculature as represented by the AASI.

What Are the Clinical Implications?

- It is now possible to link elevations in the lower limit of cerebral autoregulation with an increased AASI as determined from readily accessible intraoperative variables.
- Determination of vascular properties might be used not only to predict postoperative outcomes, but also to change perioperative management strategies in regard to ensuring adequate cerebral perfusion.

however, while easy to determine clinically, is not a robust measure of vascular stiffness and, by definition, depends directly on blood pressure. To minimize some of these shortcomings, the ambulatory arterial stiffness index (AASI) was introduced in 2006 as a noninvasive marker of arterial stiffness that is less blood pressure dependent.⁹ The AASI is defined as 1 minus the average slope of diastolic on systolic blood pressure (BP) derived from multiple BP readings that are generally obtained over 24 hours in an ambulatory setting. Moreover, the AASI accounts for variability in the relationship between the systolic and diastolic BP.¹⁰ The hypothesis is that for a given increase in diastolic BP, an increase in systolic BP is disproportionately greater in stiff arteries than in compliant ones. Therefore, a higher AASI represents a stiffer artery. Though the AASI is generally used as a marker for arterial stiffness, it is only a surrogate marker. It is not highly specific of arterial stiffness but rather of central PP.^{11–13} Studies suggest that the close univariate association between the AASI and aortic pulse wave velocity does not necessarily imply a single mechanistic link.¹⁴ In fact, it has been suggested that the AASI is influenced by peripheral vascular resistance and heart rate.¹² Moreover, a narrow range of diastolic BP values tends to flatten the regression slope and artificially increase the AASI.¹¹ This fact has led to a modified version of the AASI that derives from a symmetric regression rather than a standard regression, the symmetric AASI

(s-AASI).^{9,15} Despite its limitations, a number of studies have shown that the AASI is a reliable and independent predictor of adverse cardiovascular events in multiple populations and that it is more sensitive than PP for predicting cardiovascular events.^{10,16,17} However, the association between either the AASI or s-AASI and the pathophysiology of neurologic outcomes remains to be fully established.¹⁸ Our goal in this study was to determine the extent to which the AASI, s-AASI, or PP are associated with shifts in the LLA in patients undergoing cardiac surgery.

Methods

The data, analytic methods, and study materials will not be made available on request to other researchers for purposes of reproducing the results or replicating the procedure. This retrospective cohort study utilized data derived from patients enrolled in a previous prospective study that determined the limits of cerebral autoregulation during cardiac surgery with cardiopulmonary bypass (CPB).^{2,4,19} The protocol was approved by the Johns Hopkins Medicine Institutional Review Board (IRB00070516). Informed consent was obtained from all participants. Patients undergoing cardiac surgery with CPB were eligible for the study. We reviewed the electronic medical records between October 2009 and February 2016.

Measurements of AASI, s-AASI, and PP

We calculated the AASI, s-AASI, and peripheral PP from intraoperative continuous BP readings measured directly from the radial artery, all of which were obtained before the initiation of CPB, and recorded every 1 minute. The AASI was defined as 1 minus the regression slope of diastolic over systolic BP.⁹ If the computed AASI was outside the 0 to 1 range or R^2 of the fit was <0.2 , the AASI was not retained for further analysis. For the s-AASI, we plotted systolic BP values against diastolic BP values and assessed a linear relationship between the 2 using a symmetric regression procedure that treats both variables in a symmetric way. The resulting symmetric slope was used for the calculation of the s-AASI.⁹ The s-AASI was defined as 1 minus the symmetric regression slope as suggested by Gavish et al.⁹ PP was defined as the mean of the difference between systolic and diastolic BP.

Patient Care

All patients received routine intraoperative care, including invasive continuous radial artery pressure monitoring. Midazolam, fentanyl, and isoflurane were used for anesthesia, and vecuronium was used for muscle relaxation. Nonpulsatile flow with a target flow rate of 2.0 to 2.4 L/min per m^2 was used

for CPB. Alpha-stat pH management was performed, and oxygenation and normocapnia were ensured by continuous inline arterial blood gas monitoring with hourly calibration. The attending anesthesiologist and surgeon, who were unaware of results from LLA determination, chose the target MAP empirically based on institutional standard of care.

Limits of Cerebral Autoregulation Measurements

For each patient, bilateral middle cerebral arteries (MCAs) were monitored by transcranial Doppler ultrasonography via 2- to 2.5-MHz transducers fitted on a headband (Doppler Box, DWL; Compumedics, Charlotte, NC). Cerebral blood flow (CBF) velocity was sampled during CPB with an analog-to-digital converter at 60 Hz and then processed with ICM+ software Version 6.1 (University of Cambridge, Cambridge, UK). The signal acquisition and analysis methods have been described previously.²⁰ The mean velocity index was obtained as the moving Pearson correlation coefficient between MAP and CBF velocity.^{4,20,21} Mean velocity index values were placed in 5 mm Hg MAP bins.²⁰ The LLA was defined as the MAP at which the mean velocity index incrementally increased from <0.4 to ≥ 0.4 .^{4,21} If the mean velocity index was ≥ 0.4 for all MAPs, an impaired autoregulation pattern, the LLA was defined as the MAP at which mean velocity was the lowest. The LLA was measured separately for the left and right side of the head, and the higher value was chosen for the analysis.

Statistical Analysis

We first performed univariate linear and logistic regression analysis to assess the association between the LLA and perioperative variables, including the AASI, s-AASI, and PP. For logistic regression, the dependent variable was being a member of the population with a LLA above the median value of the LLA. Multivariate linear regression and logistic regression were then performed using a forward stepwise approach beginning with the AASI to assess the relationship between the LLA and its predictor variables. Variables from the univariate analysis that were not included in the final multivariate model were then incorporated into the model 1 at a time and the resulting model was compared with the reference multivariate model using a likelihood ratio test. The potential contribution of nonlinearity and interaction of model variables was assessed. A total sample size of 157 patients was required for the multiple linear regression to satisfy a significance level of 0.05 with power of 0.80, assuming an effect size f^2 of 0.15 (Cohen's standard medium effect size), and the number of predictors of 20 (G-power software 3.1.9.2; Faul et al, University of Kiel, Kiel, Germany).^{22,23}

The predicted LLA was calculated by using the variable from the multivariate model. Receiver-operating characteristic curves were created to determine values of the predicted LLA and the AASI or s-AASI. Outcomes of statistical tests were considered significant at $P < 0.05$, and all tests were 2-sided. Analysis was performed with Stata (Version 14, Stata Corp, College Station, TX) and Mathematica (Version 11.0, Wolfram Research Inc, Champaign, IL).

Results

LLA estimates were available from 191 subjects. However, extraction of the AASI was not possible in 10 subjects using the criteria given above. Hence, a total of 181 patients were included in the analysis. The patients' demographics and pre- and intraoperative characteristics are shown in Table 1. Of the 181 patients included, 101 (55.8%) were 70 years of age or older and 27 (14.9%) were 80 years of age or older. The transcranial Doppler-based LLA ranged from 35 mm Hg to 95 mm Hg, with a mean (SD) of 64 (13) mm Hg (Figures 1A and 1C). The LLA was >50 mm Hg in 150 (82.9%) patients. The mean (SD) of the AASI was 0.57 (0.11) and that of the s-AASI was 0.49 (0.10). The duration of intraoperative BP readings and BP variation for the determination of the s-AASI are shown in Table 2.

Both the AASI and the s-AASI were related to the LLA, with the linear fit for the AASI being superior to the one for the s-AASI ($\beta = 3.12$ mm Hg, $P < 0.001$ versus $\beta = 2.02$ mm Hg, $P < 0.022$ for each 0.1 increase; Figure 1A). Each 0.1-increment in the AASI led to a 50% increase in the odds of the LLA being above the median LLA of 65 mm Hg ($P = 0.008$, Table 3). The odds of the LLA being above the median LLA of 65 mm Hg increased by only 26% for each 0.1 increment of the s-AASI, but this relationship was not significant ($P = 0.11$, Table 3). As expected,⁹ the s-AASI was almost always lower than the AASI (Figure 1B). PP was not significantly related to the LLA, as depicted in Figure 1C ($\beta = 0.00$, $P > 0.99$).

Details on the univariate relationship between the LLA and perioperative variables are given in Table 3. The LLA was significantly associated with the AASI, parameters related to body weight, preoperative estimated glomerular filtration rate, and mean MAP throughout CPB. Neither intraoperative PP nor MAP was significantly associated with the LLA (Table 3).

The multivariate model to determine independent predictors of the LLA is presented in Table 4 ($R^2 = 0.31$). The AASI, mean MAP during CPB, and lowest body temperature were significantly associated with the LLA ($\beta = 27.6$, $P < 0.001$; $\beta = 0.62$, $P < 0.001$; $\beta = 0.95$, $P = 0.002$, respectively). Body mass index and preoperative creatinine reached statistical significance ($P = 0.01$ and 0.046 , respectively). Preoperative PP did not improve the model for LLA ($P = 0.44$). Age, sex, height, weight, prior smoking history, prior cerebrovascular accident,

Table 1. Demographics and Perioperative Characteristics

Variable	Results (n=181)
Preoperative data	
Age, y	71±8 (58–84)
Male, n (%)	123 (68.0)
PP, mm Hg	65±16 (41–98)
MAP, mm Hg	94±13 (74–115)
HR, bpm	65±15 (49–87)
Height, cm	171±10 (155–186)
Weight, kg	87±18 (60–120)
BSA, m ²	2.01±0.24 (1.62–2.42)
BMI, kg/m ²	29.6±6.1 (21.4–40.4)
Creatinine, mg/dL	1.06±0.33 (0.70–1.60)
Estimated GFR, mL/min per 1.73 m ²	72±22 (41–103)
Hb, g/dL	12.4±2.1 (8.8–15.6)
LVEF, %	52±12 (25–65)
Medical history	
CVA, n (%)	19 (10.5)
COPD, n (%)	26 (14.4)
Smoking history, n (%)	103 (56.9)
PVD, n (%)	33 (18.2)
Hypertension, n (%)	161 (89.0)
CHF, n (%)	28 (15.5)
Preoperative afib, n (%)	25 (13.8)
Diabetes mellitus, n (%)	86 (47.5)
Previous cardiac surgery, n (%)	15 (8.3)
Type of surgery	
CABG, n (%)	97 (53.6)
CABG+valve, n (%)	78 (43.1)
Valve, n (%)	6 (3.3)
Intraoperative data	
AASI	0.57±0.11 (0.39–0.75)
s-AASI	0.49±0.10 (0.29–0.64)
PP (pre-bypass mean), mm Hg	60±10 (46–77)
MAP (pre-bypass mean), mm Hg	79±8 (67–94)
HR (pre-bypass mean), bpm	65±15 (49–87)
CPB duration, min	110±47 (51–176)
Aortic cross-clamp duration, min	69±29 (32–118)
MAP during CPB, mm Hg	75±8 (64–87)
r SO ₂ mean, NIRS, %*	54±9 (39–67)
Lowest body temperature, °C	31.4±2.8 (27.0–34.7)
Highest body temperature, °C	36.4±0.9 (35.0–37.6)
LLA, mm Hg, n (%)	64±13 (45–85)

Continued

Table 1. Continued

Variable	Results (n=181)
≤50 mm Hg	31 (17.1)
>50, ≤60 mm Hg	56 (30.9)
>60, ≤70 mm Hg	37 (20.4)
>70, ≤80 mm Hg	44 (24.3)
>80 mm Hg	13 (7.2)

The results are expressed as mean±SD (95% confidence interval) or as n (%). AASI indicates ambulatory arterial stiffness index; afib, atrial fibrillation; BMI, body mass index; bpm, beats per minute; BSA, body surface area; CABG, coronary artery bypass grafting; CHF, congestive heart failure; COPD, chronic obstructive pulmonary disease; CPB, cardiopulmonary bypass; CVA, cerebrovascular accident; GFR, glomerular filtration rate; Hb, hemoglobin; HR, heart rate; LLA, lower limit of cerebral autoregulation; LVEF, left ventricular ejection fraction; MAP, mean arterial pressure; NIRS, near-infrared spectroscopy; PP, pulse pressure; PVD, peripheral vascular disease; rSO₂, regional oxygen saturation; s-AASI, symmetric ambulatory arterial stiffness index.

*Average of left- and right-sided mean rSO₂.

hypertension, and peripheral vascular disease also showed no significant association with the LLA. Using the s-AASI in a multivariate model similarly allowed us to independently predict the LLA, but to a lesser extent ($R^2=0.26$, $\beta=1.85$ per 0.1 increase in s-AASI, $P=0.017$). Using this model, only mean MAP during CPB, lowest body temperature, and body mass index were significantly related to the LLA ($\beta=0.69$, $P<0.001$; $\beta=0.91$, $P=0.004$; $\beta=-0.410.95$, $P=0.006$, respectively).

Given that the AASI had a greater association with the LLA than did the s-AASI, we decided to generate the receiver-operating characteristic curve for the AASI to predict an LLA of 65 mm Hg, which was the median LLA in our data set. The receiver-operating characteristic analysis is depicted in Figure 2. The receiver-operating characteristic curve for the AASI alone predicting an LLA above 65 mm Hg was significant (area under the curve, 0.60; 95% confidence interval, 0.51%–0.68%; $P=0.043$). Adding mean MAP during CPB and lowest body temperature improved the model (area under the curve, 0.75; 95% confidence interval, 0.68%–0.82%, $P=0.036$), but adding body mass index and preoperative creatinine had no significant effect (Figure 2, Table 4). We found no interaction between mean MAP during CPB and lowest body temperature. The s-AASI in isolation was unable to predict the LLA at 65 mm Hg (area under the curve, 0.55; 95% confidence interval, 0.46%–0.63%; $P=0.11$). Nonlinearity and interactions of the significant variables did not enhance the model performance.

Discussion

In this study of patients undergoing cardiac surgery, we investigated the relationship between the LLA and previously reported predictors of cardiovascular outcomes as quantified separately by the AASI, the s-AASI, and PP. The LLA varied

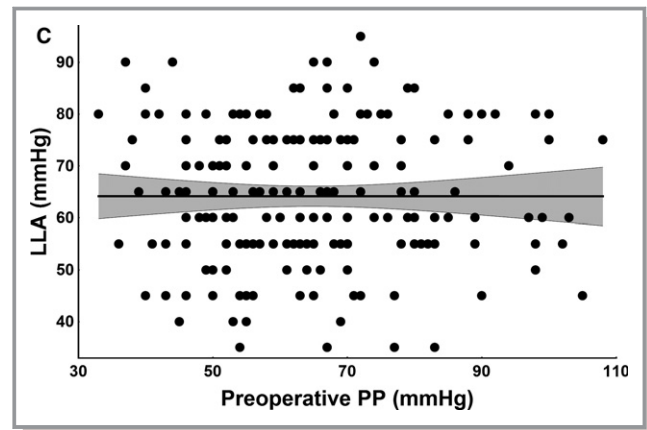
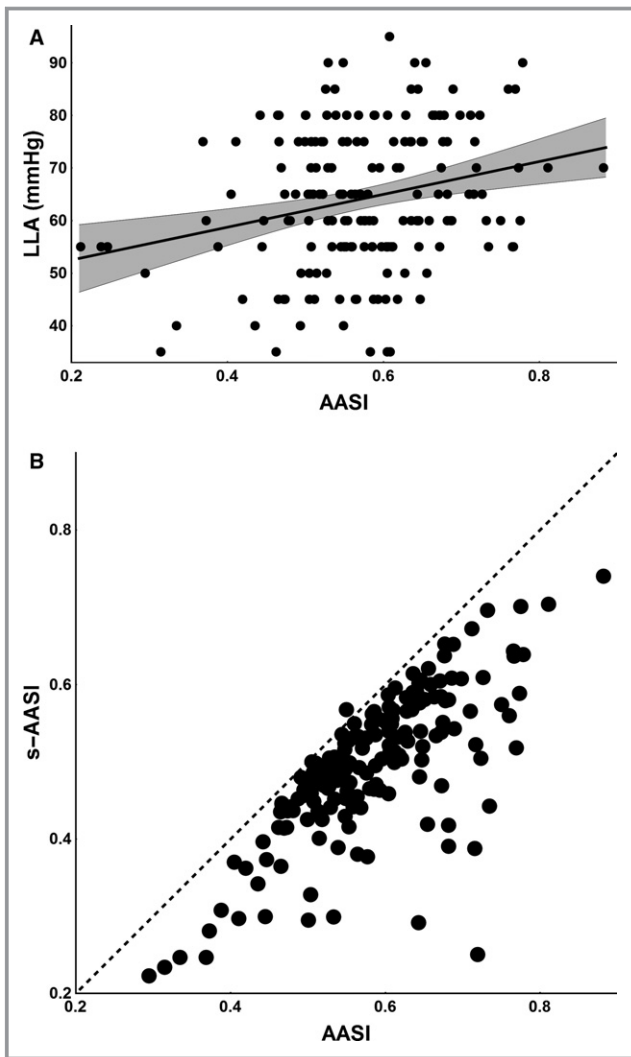


Figure 1. Continued

directly with the AASI and to a lesser extent the s-AASI, but neither PP nor MAP showed an association. These data indicate that the LLA is related to the mechanical properties of the vasculature as best represented by the AASI. Furthermore, the AASI can be used to predict threshold levels for the LLA during cardiac surgery. It is now possible to link elevations in the LLA with an increased AASI as determined from readily accessible intraoperative variables.

Cerebral arterioles match CBF and cerebral metabolic requirements by vasodilation and constriction despite changes in cerebral perfusion pressure.^{24,25} This action is referred to as cerebral pressure autoregulation. Cerebral autoregulation relies on robust cerebrovascular reactivity that leads to vasodilation when cerebral perfusion pressure decreases and vasoconstriction when it increases.²⁶ The cerebrovascular endothelium, perivascular nerves, and

Figure 1. Relationship between the lower limit of cerebral autoregulation (LLA) and several measures of vascular properties. A, Scatter plot of the distribution of the LLA and the corresponding ASSI. The linear fit between the 2 ($\beta=3.12$ mm Hg per 0.1 increase in ASSI, $P<0.001$) and related 95% confidence intervals is also shown. Each 0.1 increment in the AASI increased the odds of the LLA being above the median LLA value of 65 mm Hg by 50% ($P=0.008$, Table 3). In contrast, the fit between the LLA and the s-AASI (not shown) was less compelling ($\beta=2.02$ mm Hg per 0.1 increase in s-AASI, $P=0.029$, Table 3), and the ability to use the s-AASI to determine whether the LLA is elevated diminished. The odds of the LLA being above the median LLA value of 65 mm Hg increased by only 26% for each 0.1 increment of the s-AASI, but this relationship was not significant ($P=0.17$). B, The relationship between the AASI and s-AASI, along with the corresponding line-of-identity, illustrates that the s-AASI is virtually always lower than the AASI, thereby reducing the apparent stiffness of the associated vasculature. C, Scatter plot of the distribution of the LLA and the corresponding preoperative pulse pressure (PP). The linear fit between the 2 ($\beta=0.00$, $P>0.99$) and 95% confidence intervals are also shown. The use of mean intraoperative pre-bypass PP (not shown) was similarly unrelated to the LLA ($\beta=0.07$, $P=0.35$). AASI indicates ambulatory arterial stiffness index; s-AASI, symmetric ambulatory arterial stiffness index.

Table 2. Intraoperative Continuous Pre-CPB BP Measurement for the Determination of the AASI

Variable	Median	IQR
Maximum SBP, mm Hg	176	160–200
Median SBP, mm Hg	114	108–122
Minimum SBP, mm Hg	74	66–80
Range of SBP, mm Hg	100	86–124
Maximum DBP, mm Hg	92	80–104
Median DBP, mm Hg	56	50–60
Minimum DBP, mm Hg	38	32–42
Range of DBP, mm Hg	52	44–64
Duration of BP measurement, min	140	114–168

AASI indicates ambulatory arterial stiffness index; BP indicates blood pressure; CPB, cardiopulmonary bypass; DBP, diastolic blood pressure; IQR, interquartile range; SBP, systolic blood pressure.

Table 3. Univariate Analysis of the Relationship Between the LLA and Perioperative Variables for Both Linear (β) and Logistic (OR for LLA >65 mm Hg) Regression

Variable	β (95% CI)	P Value	OR (95% CI)	P Value
Preoperative data				
Age	-0.04 (-0.20 to 0.21)	0.75	1.00 (0.96-1.04)	0.95
Male	0.14 (-4.07 to 4.34)	0.95	0.69 (0.36-1.29)	0.24
PP	0.00 (-0.08 to 0.23)	>0.99	1.00 (0.98-1.02)	0.92
MAP	0.07 (-0.08 to 0.23)	0.35	1.01 (0.98-1.03)	0.49
HR	-0.06 (-0.19 to 0.08)	0.40	0.98 (0.96-1.00)	0.11
Height	0.08 (-0.11 to 0.27)	0.42	1.00 (0.97-1.03)	0.92
Weight	-0.15 (-0.26 to -0.05)	0.005*	0.98 (0.97-1.00)	0.041*
BSA	-10.7 (-18.7 to -2.7)	0.009*	0.26 (0.072-0.93)	0.038*
BMI	-0.59 (-0.90 to -0.27)	<0.001*	0.94 (0.89-0.99)	0.020*
Prior CVA	1.5 (-4.9 to 7.9)	0.48	1.09 (0.41-2.84)	0.87
Hypertension	3.3 (-3.0 to 9.5)	0.31	1.29 (0.49-3.41)	0.61
PVD	1.8 (-3.1 to 7.1)	0.77	1.29 (0.60-2.77)	0.51
Diabetes mellitus	0.1 (-3.9 to 4.0)	0.97	1.03 (0.57-1.87)	0.92
CHF	-1.7 (-7.2 to 3.7)	0.53	0.79 (0.34-1.83)	0.59
COPD	0.3 (-5.3 to 5.9)	0.91	1.10 (0.47-2.55)	0.82
Smoking history	-0.3 (-4.2 to 3.7)	0.90	0.95 (0.52-1.73)	0.87
Afib	0.03 (-5.4 to 6.0)	0.92	1.19 (0.51-2.79)	0.69
Creatinine	-4.4 (-10.4 to 1.6)	0.15	0.68 (0.26-1.75)	0.43
GFR	0.098 (0.009 to 0.188)	0.032*	1.01 (0.99, 1.02)	0.28
Hb	-0.01 (-0.96 to 0.94)	0.98	1.02 (0.88-1.18)	0.78
LVEF	-0.02 (-0.18 to 0.14)	0.82	1.00 (0.98-1.03)	0.77
Intraoperative data				
AASI	3.12 (1.43-4.82) [†]	<0.001*	1.50 (1.11-2.02) [†]	0.008*
s-AASI	2.02 (2.90-3.74) [†]	0.022*	1.26 (0.95-1.67) [†]	0.11
Pre-bypass PP, mm Hg	0.09 (-0.10 to 0.29)	0.35	1.01 (0.98-1.04)	0.52
Pre-bypass MAP, mm Hg	-0.16 (-0.40 to 0.08)	0.19	0.99 (0.95-1.02)	0.42
Pre-bypass HR, bpm	-0.06 (-0.19 to 0.08)	0.39	0.98 (0.96-1.00)	0.11
CPB duration	-0.05 (-0.09 to -0.00)	0.033*	0.99 (0.99-1.00)	0.12
Aortic cross-clamp duration	-0.06 (-0.12 to 0.01)	0.10	0.99 (0.98-1.01)	0.32
MAP during CPB	0.73 (0.50-0.97)	<0.001*	1.12 (1.06-1.17)	<0.001*
rSO ₂ mean	0.01 (-0.20 to 0.22)	0.93	1.01 (0.98-1.04)	0.54
Lowest body temperature	0.65 (-0.06 to 1.34)	0.07	1.09 (0.98-1.22)	0.12
Highest body temperature	-0.22 (-2.4 to 1.96)	0.84	0.90 (0.65-1.25)	0.53

AASI indicates ambulatory arterial stiffness index; Afib, atrial fibrillation; BMI, body mass index; bpm, beats per minute; BSA, body surface area; CHF, congestive heart failure; CI, confidence interval; COPD, chronic obstructive pulmonary disease; CPB, cardiopulmonary bypass; CVA, cerebrovascular accident; GFR, glomerular filtration rate; Hb, hemoglobin; HR, heart rate; LLA, lower limit of cerebral autoregulation; LVEF, left ventricular ejection fraction; MAP, mean arterial pressure; OR, odds ratio; PP, pulse pressure; PVD, peripheral vascular disease; rSO₂, regional oxygen saturation; s-AASI, symmetric ambulatory arterial stiffness index.

* $P < 0.05$.

[†]For both linear and logistic regression, the AASI and s-AASI were multiplied by 10 so that β and the OR represent the increase per 0.1 U of either.

vascular smooth muscle cells play distinct roles in the regulation of CBF.²⁵ It is well known that an acute drop in arterial BP induces a decrease in cerebral vascular tone,²⁷

whereas increased cerebral flow velocity induces cerebral vasoconstriction.²⁵ From a physiological point of view, the LLA represents the point of maximal cerebrovascular dilation.

Table 4. Multivariate Linear and Logistic Regression to Determine Independent Predictors of the LLA*

Variable	β (95% CI) [†]	<i>P</i> Value [‡]	OR (95% CI)	<i>P</i> Value
Intercept	−23.0 (−52.7 to 6.6)	0.127	0.000 (0.00–0.00)	<0.001 [‡]
AASI	2.76 (1.26–4.26) [§]	<0.001 [‡]	1.52 (1.09–2.12)	0.013 [‡]
MAP (mean during bypass)	0.62 (0.40–0.85)	<0.001 [‡] (<0.001)	1.12 (1.06–1.18)	<0.001 [‡] (<0.001)
Lowest body temperature	0.95 (0.35–1.56)	0.002 [‡] (0.004)	1.15 (1.02–1.31)	0.022 [‡] (0.019)
BMI	−0.38 (−0.66 to −0.09)	0.010 [‡] (0.010)		0.18
Preoperative creatinine	0.079 (0.001–0.156)	0.046 [‡] (0.042)		0.42
Age		0.20		
Male		0.56		
Preoperative PP		0.44		
Preoperative MAP		0.49		
Preoperative HR		0.22		
Height		0.69		
Weight		0.56		
BSA		0.91		
Prior CVA		0.52		
Hypertension		0.53		
PVD		0.52		
Diabetes mellitus		0.79		
CHF		0.91		
COPD		0.95		
Smoking history		0.25		
Preoperative afib		0.53		
Preoperative Hb		0.08		
Preoperative LVEF		0.72		
Pre-bypass PP		0.33		
Pre-bypass MAP		0.26		
Pre-bypass HR		0.20		
CPB duration		0.56		
Aortic cross-clamp duration		0.50		
rSO ₂ mean		0.57		
Highest body temperature		0.49		

The logistic model evaluated whether the LLA was >65 mm Hg, its median value. AASI indicates ambulatory arterial stiffness index; afib, atrial fibrillation; BMI, body mass index; BSA, body surface area; CHF, congestive heart failure; CI, confidence interval; COPD, chronic obstructive pulmonary disease; CPB, cardiopulmonary bypass; CVA, cerebrovascular accident; Hb, hemoglobin; HR, heart rate; LLA, lower limit of cerebral autoregulation; LVEF, left ventricular ejection fraction; MAP, mean arterial pressure; OR, odds ratio; PP, pulse pressure; PVD, peripheral vascular disease; rSO₂, regional oxygen saturation.

* $R^2=0.31$, $P<0.001$.

[†]The 95% CI and *P* values for significant variables (‡) are given for the included variables for the multivariate model at the top. *P* values below these (in parentheses) indicate the significance of the model generated by the addition of the given variable without including any of those below using a likelihood ratio test. The *P* values for the variables listed below those deemed to be significant indicate the significance of any improvement as indicated by a likelihood ratio test between the multivariate model and one that incorporates just the additional variable. For each of the variables found to be significant in the multivariate model, the potential contribution of nonlinear terms was considered (not shown). Furthermore, the significance of interactions between the variables in the multivariate model was also considered. In no instance did the inclusion of nonlinearities or interactions contribute to the model.

[§]For both linear and logistic regression, the AASI was multiplied by 10 so that β and the OR represents the increase per 0.1 U of the AASI.

It has been reported that a direct relationship exists between the AASI and central PP.²⁸ A close relationship between aortic vascular stiffness, pressure pulsatility, cerebral microvascular function, and brain damage has also been

suggested.^{29–32} Moreover, microvascular structure and function are altered in the presence of excessive pressure pulsatility resulting from increased large artery stiffness.³² Therefore, when the heart contracts, the forward pressure

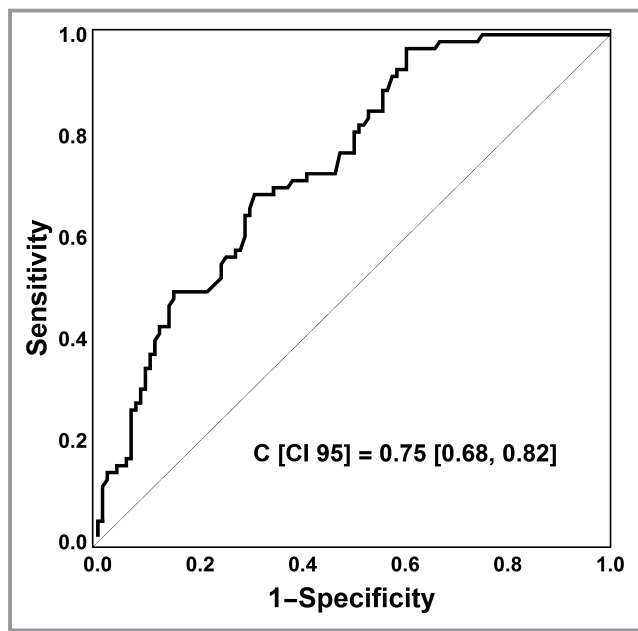


Figure 2. Assessment of the AASI to predict the lower limit of cerebral autoregulation (LLA). Receiver operating characteristic curve of the AASI for predicting that the measured LLA is above the threshold of 65 mm Hg using the multivariate logistic model of Table 4. The model is able to predict a LLA with high specificity but relatively low sensitivity. The area under the curve is 0.75 (95% CI, 0.68%–0.82%, $P=0.036$). AASI indicates ambulatory arterial stiffness index; CI indicates confidence interval.

wave travels from the heart to the aorta until it encounters regions of impedance mismatch caused by variable vessel wall properties and diameter. This mismatch produces a partial wave reflection, which is helpful for the periphery because less pulsatile energy is transmitted distally to the microcirculation. However, as the large arteries stiffen, this impedance mismatch is reduced, which decreases the wave reflection and facilitates transmission of excessive pulsatile energy into the microcirculation.^{30,32} Furthermore, the stiffer aorta described by increasing pulse wave velocity leads to an early return of the reflected wave, which increases systolic BP, whereas diastolic BP is not changed.³¹ Thus, central PP and pressure pulsatility are increased. In fact Webb et al³³ reported that greater MCA pulsatility was independently associated with higher aortic PP. It is therefore conceivable that increased pressure pulsatility may trigger microvascular remodeling that limits CBF because the remodeled microvascular lumen area is reduced even when maximally vasodilated.³⁰ Microvascular remodeling is also associated with increased myogenic tone and impaired vasomotor reactivity, both of which might directly influence the limit of CBF autoregulation and increase susceptibility to focal ischemia.³¹ Given that the amount of blood flow is greater in compliant arteries with a low pressure pulsatility,^{34,35} the LLA should be lower in patients with a compliant vasculature

than in those with one that is more stiff. It has been postulated before and commonly assumed that the LLA is elevated in patients with hypertension.³⁶ Although excessive pulsatility is associated with hypertension,^{28,37} our results indicate that the AASI is a more sensitive marker of increased LLA than peripheral PP or MAP.

Our findings are consistent with those of Joshi et al⁴ in that we observed no relationship between preoperative MAP and LLA. As with the previous study, we showed that LLA ranged from 35 mm Hg to 95 mm Hg in patients during cardiac surgery. In contrast to that study, however, we found relationships between the AASI and the s-AASI, and cerebral autoregulation. Although the s-AASI was significantly associated with the LLA, the relationship was not as strong as that between the AASI and LLA. Furthermore, the AASI appears to be a better predictor of the LLA than the s-AASI is. Our findings suggest that the LLA is dependent not only on the AASI but also on intraoperative vital signs such as MAP during CPB and the lowest body temperature. The latter relationships may be because of an epiphenomenon as both are chosen intraoperatively by the surgical team. Even though the surgical team was blinded to the LLA measurements, they could have chosen a higher MAP for patients on bypass who subjectively appeared to have an altered LLA, such as those who had hypertension that was difficult to control intraoperatively or those who appeared frail. Prior studies have shown that the duration and magnitude of BP below the LLA is associated with acute kidney injury³⁸ and major morbidity and mortality² after cardiac surgery. Those studies suggested that maintaining MAP within the range of cerebral autoregulation may improve postoperative outcomes. The measurement of AASI might be able to change perioperative management strategies as we predict BP targets based on the AASI to ensure that MAP remains above the LLA.

Finally, it has been reported that the AASI, the s-AASI, and PP are independent predictors of cardiovascular mortality after adjustment for other risk factors in various populations.^{18,39} Moreover, some studies compared the prognostic ability of AASI with that of PP. Dolan et al¹⁰ reported that the AASI was more predictive of cardiovascular mortality and fatal stroke than PP was, especially in normotensive subjects. Muxfeldt et al¹⁷ reported that the AASI was superior to ambulatory PP as a cardiovascular risk marker in resistant hypertensive patients. Our finding of the independent relationship between the AASI and the LLA supports and complements these previous studies. One possible reason that the AASI is more predictive of the LLA is that it provides relatively more information about the structural and functional characteristics of the arteries, whereas PP is more strongly dependent on BP.¹⁰ However, in the current study we did not assess the prognostic ability of either variable; rather, we focused on the relationship between the AASI and the LLA.

The association between the 2 suggests an underlying physical basis for the LLA, with stiffer vessels requiring higher pressures to maintain cerebral perfusion, a hypothesis consistent with the mechanism of pulsatile blood flow in compliant vessels. Additional studies are necessary to assess the prognostic ability of the AASI beyond cardiac surgical patients.

An advantage of this study is that we determined the AASI from continuous intraoperative BP measurements. Even though this is not a 24-hour recording, the nature of cardiac surgery is that BPs traverse a rather large range over a relatively short interval. However, limitations of our study include the fact that the AASI is largely influenced by peripheral vascular resistance and stroke volume (decrease in peripheral vascular resistance and/or stroke volume with an increase in the AASI), which we did not assess in this study.^{12,13} The AASI, which was initially introduced as a marker for vascular stiffness, is now considered to be more representative of central PP and tends to overestimate the relationship between systolic and diastolic BP, hence the introduction of the s-AASI that uses a symmetric regression. However, in our data set, the AASI was a better predictor of the LLA than was the s-AASI. This finding could be explained by the fact that we were primarily evaluating inherent vascular properties, including, but not limited to, vascular stiffness, in a very homogeneous patient population under hemodynamically controlled circumstances. One downside of the AASI is that it does not detect nondipper hypertensive patients. We did not identify such patients in our data set because we did not perform a 24-hour evaluation, which would have included the circadian dip in BP. Many medications used during cardiac surgery (especially the anesthetics) can modulate peripheral resistance and stroke volume, and thereby increase the AASI. Thus, such medications may introduce a systemic bias for determination of the AASI. It should be noted also that blood velocity measurements by transcranial Doppler ultrasonography reflect volumetric blood flow only if the cross-sectional area of the MCA remains constant. Any changes in arterial diameter can introduce errors in the estimation of flow. Though Serrador et al⁴⁰ demonstrated that the diameter of the MCA does not change in humans at the level of measurement during hyper/hypocapnia or during moderate hypotension, the effects of BP changes on MCA diameter have not been fully investigated.⁴¹ Finally, we did not measure central PP; rather, we measured PP from the radial artery. Therefore, we did not assess the effect of central PP on the cerebral autoregulation in this study.

Conclusions

We investigated the relationship between the LLA and vascular properties as quantified separately by the

intraoperative AASI, the s-AASI, and PP in patients undergoing cardiac surgery. The AASI was able to predict the LLA with a greater ability than the s-AASI in such patients, but PP had no predictive ability. We found that the likelihood of a LLA >65 mm Hg increases by 50% for every 0.1 increase in the AASI. Thus, the AASI is significantly associated with changes in cerebral autoregulation. Our findings suggest an underlying physical basis for the LLA, with stiffer vessels requiring higher pressures to maintain cerebral perfusion. It is now possible to link elevations in the LLA with an increased AASI as determined from readily accessible perioperative variables and to predict the LLA from those variables. This study therefore emphasizes the importance of the AASI to intraoperative management and, together with the expanding literature on vascular stiffness and adverse outcomes, suggests that vascular stiffness should be added to our armamentarium of preoperative evaluation. Sophisticated determination of vascular function might therefore be used not only to predict postoperative outcomes, but also to change perioperative management strategies such as BP targets to ensure that patient MAP remains above the LLA.

Sources of Funding

This study was supported in part by a grant from the National Heart, Lung, and Blood Institute (R01 HL 092259-09) to Dr Hogue.

Disclosures

None.

References

1. Van Wermeskerken GK, Lardenoye JWH, Hill SE, Grocott HP, Phillips-Bute B, Smith PK, Reves JG, Newman MF. Intraoperative physiologic variables and outcome in cardiac surgery: part II. Neurologic outcome. *Ann Thorac Surg.* 2000;69:1077–1083.
2. Ono M, Brady K, Easley RB, Brown C, Kraut M, Gottesman RF, Hogue CW. Duration and magnitude of blood pressure below cerebral autoregulation threshold during cardiopulmonary bypass is associated with major morbidity and operative mortality. *J Thorac Cardiovasc Surg.* 2014;147:483–489.
3. Lassen NA. Cerebral blood flow and oxygen consumption in man. *Physiol Rev.* 1959; 39:183–238.
4. Joshi B, Ono M, Brown C, Brady K, Easley RB, Yenokyan G, Gottesman RF, Hogue CW. Predicting the limits of cerebral autoregulation during cardiopulmonary bypass. *Anesth Analg.* 2012;114:503–510.
5. Bucerius J, Gummert JF, Borger MA, Walther T, Doll N, Onnasch JF, Metz S, Falk V, Mohr FW. Stroke after cardiac surgery: a risk factor analysis of 16,184 consecutive adult patients. *Ann Thorac Surg.* 2003;75:472–478.
6. Glasser SP, Halberg DL, Sands CD, Mosher A, Muntner PM, Howard G. Is pulse pressure an independent risk factor for incident stroke, reasons for geographic and racial differences in stroke. *Am J Hypertens.* 2015;28:987–994.
7. Laurent S, Katsahian S, Fassot C, Tropeano AI, Gautier I, Laloux B, Boutouyrie P. Aortic stiffness is an independent predictor of fatal stroke in essential hypertension. *Stroke.* 2003;34:1203–1206.
8. Benjo A, Thompson RE, Fine D, Hogue CW, Alejo D, Kaw A, Gerstenblith G, Shah A, Berkowitz DE, Nyhan D. Pulse pressure is an age-independent predictor of stroke development after cardiac surgery. *Hypertension.* 2007;50:630–635.

9. Gavish B, Ben-Dov IZ, Bursztyn M. Linear relationship between systolic and diastolic blood pressure monitored over 24 h: assessment and correlates. *J Hypertens*. 2008;26:199–209.
10. Dolan E, Thijs L, Li Y, Atkins N, McCormack P, McClory S, O'Brien E, Staessen JA, Stanton AV. Ambulatory arterial stiffness index as a predictor of cardiovascular mortality in the Dublin Outcome Study. *Hypertension*. 2006;47:365–370.
11. Schillaci G, Parati G, Pirro M, Pucci G, Mannarino MR, Sperandini L, Mannarino E. Ambulatory arterial stiffness index is not a specific marker of reduced arterial compliance. *Hypertension*. 2007;49:986–991.
12. Kips JG, Vermeersch SJ, Reymond P, Boutouyrie P, Stergiopoulos N, Laurent S, Van Bortel LM, Segers P. Ambulatory arterial stiffness index does not accurately assess arterial stiffness. *J Hypertens*. 2012;30:574–580.
13. Westerhof N, Lankhaar JW, Westerhof BE. Ambulatory arterial stiffness index is not a stiffness parameter but a ventriculo-arterial coupling factor. *Hypertension*. 2007;49:e7.
14. Laurent S. Surrogate measures of arterial stiffness: do they have additive predictive value or are they only surrogates of a surrogate? *Hypertension*. 2006;47:325–326.
15. Schillaci G, Parati G. Ambulatory arterial stiffness index: merits and limitations of a simple surrogate measure of arterial compliance. *J Hypertens*. 2008;26:182–185.
16. Hansen TW, Staessen JA, Torp-Pedersen C, Rasmussen S, Li Y, Dolan E, Thijs L, Wang J-G, O'Brien E, Ibsen H, Jeppesen J. Ambulatory arterial stiffness index predicts stroke in a general population. *J Hypertens*. 2006;24:2247–2253.
17. Muxfeldt ES, Cardoso CRL, Dias VB, Nascimento ACM, Salles GF. Prognostic impact of the ambulatory arterial stiffness index in resistant hypertension. *J Hypertens*. 2010;28:1547–1553.
18. Kollias A, Stergiou GS, Dolan E, O'Brien E. Ambulatory arterial stiffness index: a systematic review and meta-analysis. *Atherosclerosis*. 2012;224:291–301.
19. Ono M, Joshi B, Brady K, Easley RB, Zheng Y, Brown C, Baumgartner W, Hogue CW. Risks for impaired cerebral autoregulation during cardiopulmonary bypass and postoperative stroke. *Br J Anaesth*. 2012;109:391–398.
20. Brady K, Joshi B, Zweifel C, Smielewski P, Czosnyka M, Easley RB, Hogue CW. Real-time continuous monitoring of cerebral blood flow autoregulation using near-infrared spectroscopy in patients undergoing cardiopulmonary bypass. *Stroke*. 2010;41:1951–1956.
21. Ono M, Zheng Y, Joshi B, Sigl JC, Hogue CW. Validation of a stand-alone near-infrared spectroscopy system for monitoring cerebral autoregulation during cardiac surgery. *Anesth Analg*. 2013;116:198–204.
22. Faul F, Erdfelder E, Buchner A, Lang A-G. Statistical power analyses using G*Power 3.1: tests for correlation and regression analyses. *Behav Res Methods*. 2009;41:1149–1160.
23. Cohen J. A power primer. *Psychol Bull*. 1992;112:155–159.
24. Rhee CJ, Kibler KK, Easley RB, Andropoulos DB, Smielewski P, Brady KM, Czosnyka M. Renovascular reactivity measured by near-infrared spectroscopy. *J Appl Physiol*. 2012;113:307–314.
25. Peterson EC, Wang Z, Britz G. Regulation of cerebral blood flow. *Int J Vasc Med*. 2011;2011:823525.
26. Meng L, Gelb AW. Regulation of cerebral autoregulation by carbon dioxide. *Anesthesiology*. 2015;122:196–205.
27. Donnelly J, Budohoski KP, Smielewski P, Czosnyka M. Regulation of the cerebral circulation: bedside assessment and clinical implications. *Crit Care*. 2016;20:129.
28. Li Y, Wang J, Dolan E, Gao P-J, Guo H-F, Nawrot T, Alice V, Zhu D, Brien EO, Staessen JA, Stanton AV, Zhu D, O'Brien E, Staessen JA. Ambulatory arterial stiffness index derived from 24-hour ambulatory blood pressure monitoring. *Hypertension*. 2006;47:359–364.
29. O'Rourke MF, Safar ME. Relationship between aortic stiffening and microvascular disease in brain and kidney: cause and logic of therapy. *Hypertension*. 2005;46:200–204.
30. Mitchell GF, Van Buchem MA, Sigurdsson S, Gotal JD, Jonsdottir MK, Kjartansson Ó, Garcia M, Aspelund T, Harris TB, Gudnason V, Launer LJ. Arterial stiffness, pressure and flow pulsatility and brain structure and function: the Age, Gene/Environment Susceptibility-Reykjavik study. *Brain*. 2011;134:3398–3407.
31. Tzourio C, Laurent S, Debette S. Is hypertension associated with an accelerated aging of the brain? *Hypertension*. 2014;63:894–903.
32. Mitchell GF. Effects of central arterial aging on the structure and function of the peripheral vasculature: implications for end-organ damage. *J Appl Physiol*. 2008;105:1652–1660.
33. Webb AJS, Simoni M, Mazzucco S, Kuker W, Schulz U, Rothwell PM. Increased cerebral arterial pulsatility in patients with leukoaraiosis: arterial stiffness enhances transmission of aortic pulsatility. *Stroke*. 2012;43:2631–2636.
34. Womersley JR. XXIV. Oscillatory motion of a viscous liquid in a thin-walled elastic tube—I: the linear approximation for long waves. *Lond Edinb Dubl Phil Mag*. 1955;46:199–221.
35. Niroomand Oscuii H, Tafazzoli Shadpour M, Ghalichi F. Flow characteristics in elastic arteries using a fluid-structure interaction model. *Am J Appl Sci*. 2007;4:516–524.
36. Pires PW, Dams Ramos CM, Matin N, Dorrance AM. The effects of hypertension on the cerebral circulation. *Ann Clin Lab Sci*. 1991;21:147–152.
37. Sun Z. Aging, arterial stiffness, and hypertension. *Hypertension*. 2015;65:252–256.
38. Ono M, Arnaoutakis GJ, Fine DM, Brady K, Easley RB, Zheng Y, Brown C, Katz NM, Grams ME, Hogue CW. Blood pressure excursions below the cerebral autoregulation threshold during cardiac surgery are associated with acute kidney injury. *Crit Care Med*. 2013;41:464–471.
39. Benetos A, Rudnichi A, Safar M, Guize L. Pulse pressure and cardiovascular mortality in normotensive and hypertensive subjects. *Hypertension*. 1998;32:560–564.
40. Serrador JM, Picot PA, Rutt BK, Shoemaker JK, Bondar RL. MRI measures of middle cerebral artery diameter in conscious humans during simulated orthostasis. *Stroke*. 2000; 31:1672–1678.
41. Brothers MR, Zhang R. CrossTalk opposing view: the middle cerebral artery diameter does not change during alterations in arterial blood gases and blood pressure. *J Physiol*. 2016;594:4077–4079.



Relationship Between the Ambulatory Arterial Stiffness Index and the Lower Limit of Cerebral Autoregulation During Cardiac Surgery

Yurie Obata, Viachaslau Barodka, Dan E. Berkowitz, Allan Gottschalk, Charles W. Hogue and Jochen Steppan

J Am Heart Assoc. 2018;7:e007816; originally published February 8, 2018;

doi: 10.1161/JAHA.117.007816

The *Journal of the American Heart Association* is published by the American Heart Association, 7272 Greenville Avenue, Dallas, TX 75231
Online ISSN: 2047-9980

The online version of this article, along with updated information and services, is located on the World Wide Web at:

<http://jaha.ahajournals.org/content/7/4/e007816>

Subscriptions, Permissions, and Reprints: The *Journal of the American Heart Association* is an online only Open Access publication. Visit the Journal at <http://jaha.ahajournals.org> for more information.